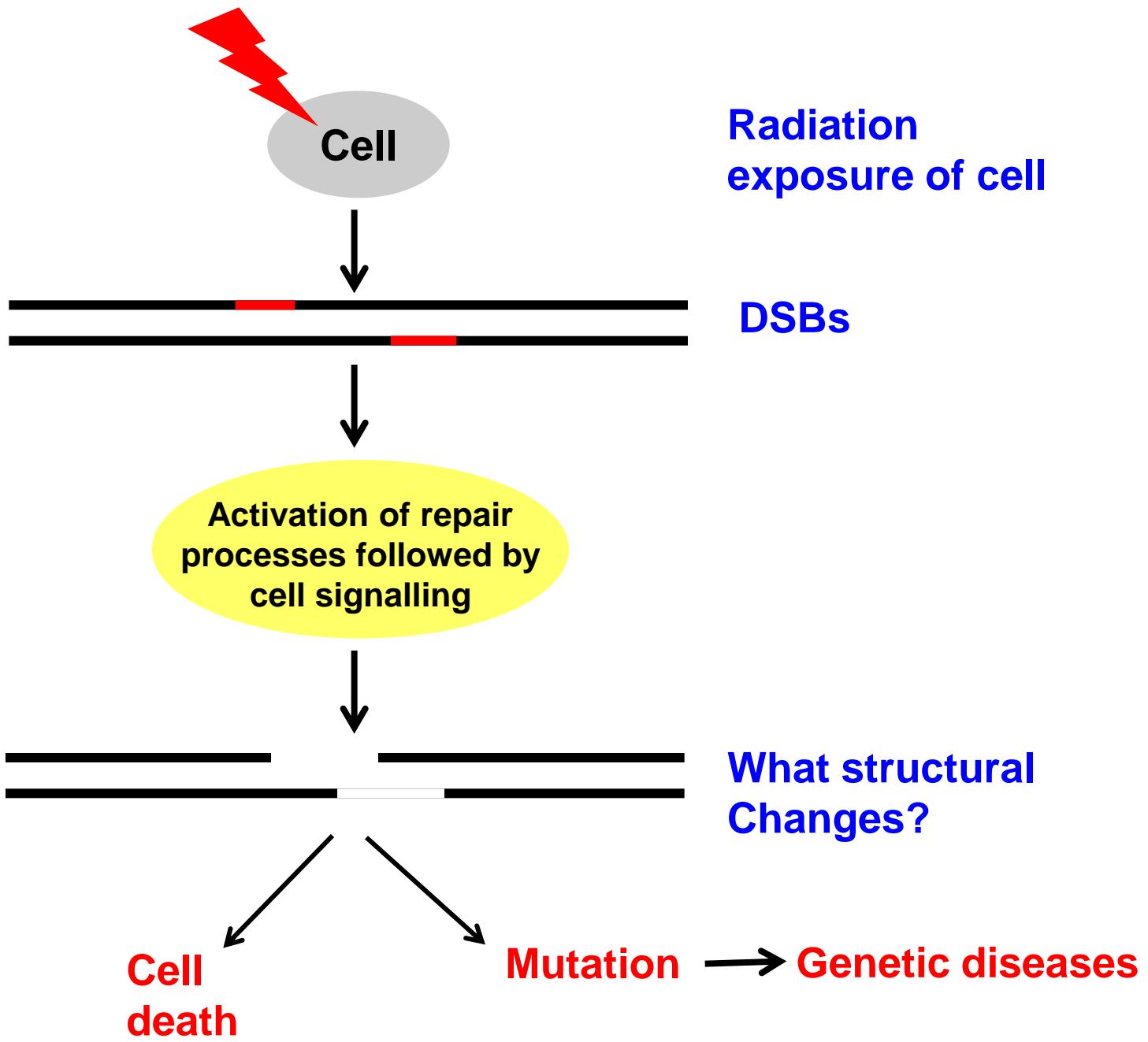


***Microdosimetry* in radiation protection & radiation therapy**

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Department of Oncology-Pathology,
Karolinska Institutet



Some Questions

- In Radiation Physics

- Characterization of radiation field

- Accurate dosimetry

- In Radiation Protection

- Background levels for risk estimation (genetic & cancer)

- In Radiation therapy

- Clinical RBE values

- In Radiation Biology

- Mechanism of radiation induced DNA Damage Response & Repair

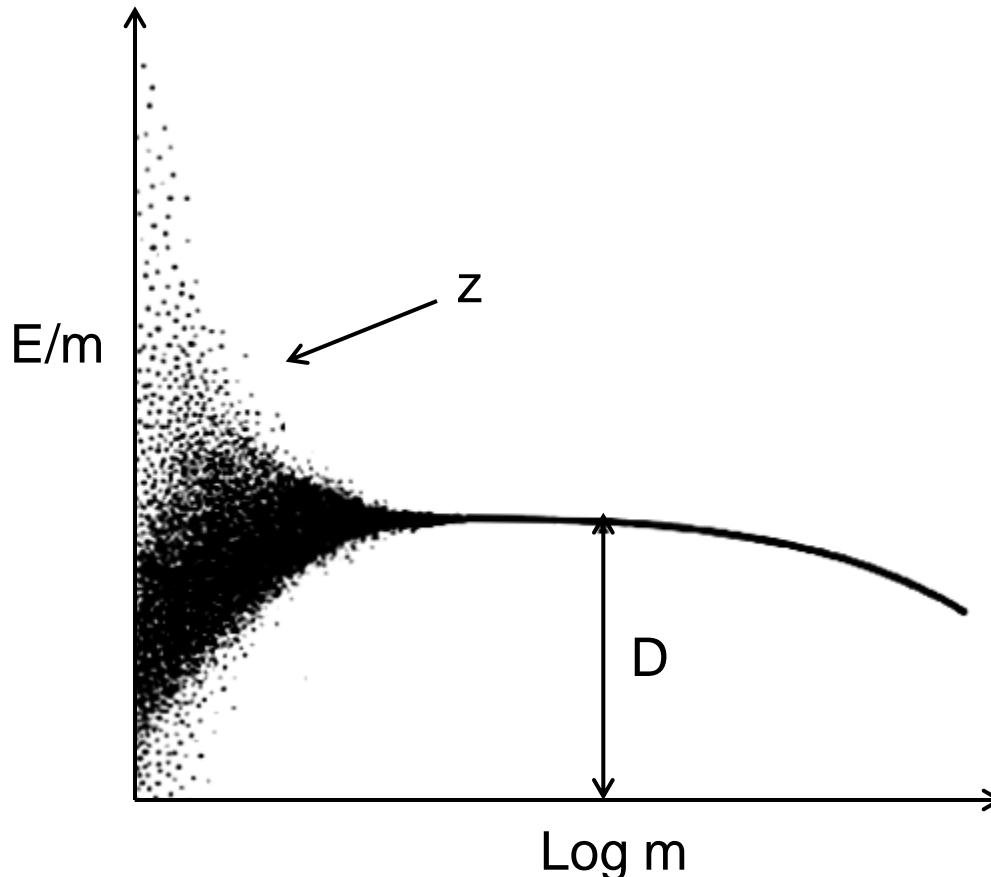
- What is the relevant type of damage induced by IR?

Hypothesis

Progress in radiation risk estimation and cancer therapy in the 21st century will be driven by the integration of genomic knowledge with that of DNA Damage, and DNA-repair mechanism

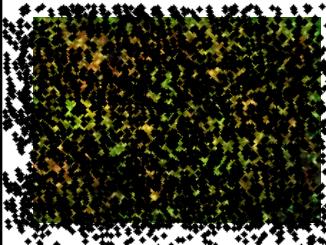
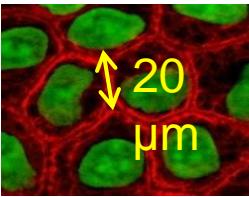
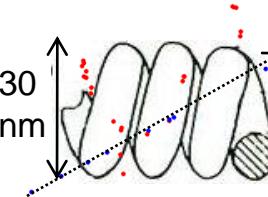
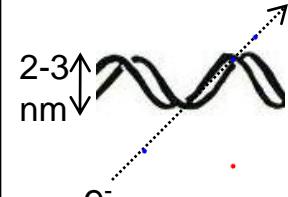
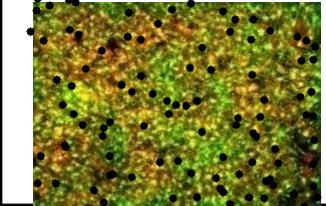
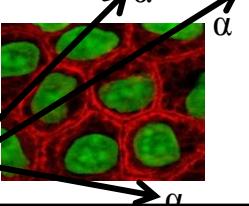
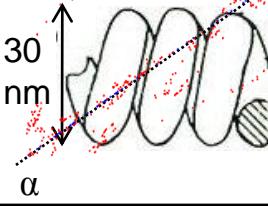
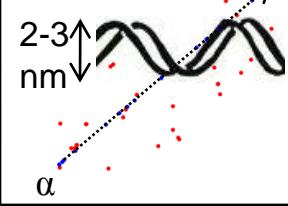
Most radiation-induced mutations are large multi-gene deletions

Spontaneous deletions induced in germ cells are more likely to be multi-system developmental abnormalities rather than single gene diseases



Energy density as a function of the mass for which energy density is determined. The horizontal line covers the region in which the absorbed dose can be established in a single measurement. Rossi 1968

Microscopic consequences of 1cGy absorbed dose

Radiation	Tissue	Cells	Chromatin fibre	DNA	Mean no. lethal lesions per cell
γ -ray					
Dose uniformity	Uniform dose=1 cGy	\sim Uniform dose \sim 1 cGy	very non-uniform	very non-uniform	
Mean no. tracks	$\sim 10^{11} \text{ gm}^{-1}$	$\sim 5000 \text{ cell}^{-1}$	$\sim 10^{-6} \text{ segment}^{-1}$	$\sim 10^{-6} \text{ segment}^{-1}$	
^{220}Rn 2-4 α particles					
Dose uniformity	0 - 2 cGy	0 - ~ 30 cGy	0 - $\sim 10^4$ Gy	0- 2×10^6 Gy	
Mean no. tracks	$\sim 10^7 \text{ gm}^{-1}$	$\sim 0.26 \text{ cell}^{-1}$ $\sim 90\%$ of cells unirradiated	$\sim 6 \times 10^{-7} \text{ segment}^{-1}$	$\sim 10^{-9} \text{ segment}^{-1}$	

Why Microdosimetry

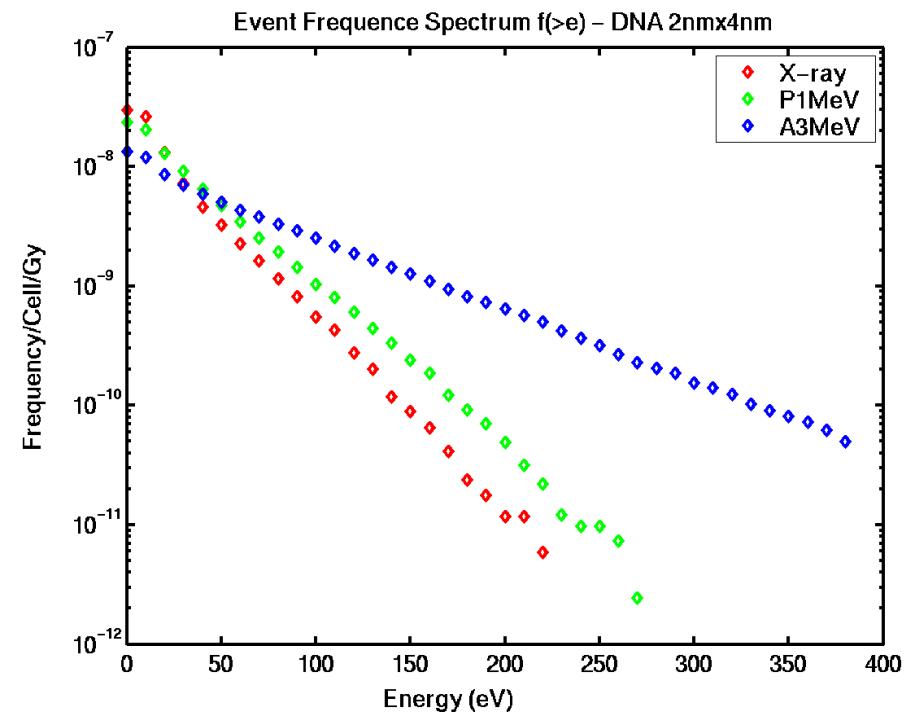
1. Dosimetry at a microscopic scale
 - Densely ionising radiation → dose inhomogeneity at cellular/subcellular levels
 - Dose calculations based on stopping power are inaccurate at a sub-mm precision.
2. Effective method to characterise the radiation quality of ion beams
 - Linear Energy Transfer (LET): average and macroscopic quantity → insufficient as a descriptor of biological effectiveness
 - Better alternative: a quantity related to energy depositions at a scale relevant to biological targets → **Microdosimetry**

Why Microdosimetry

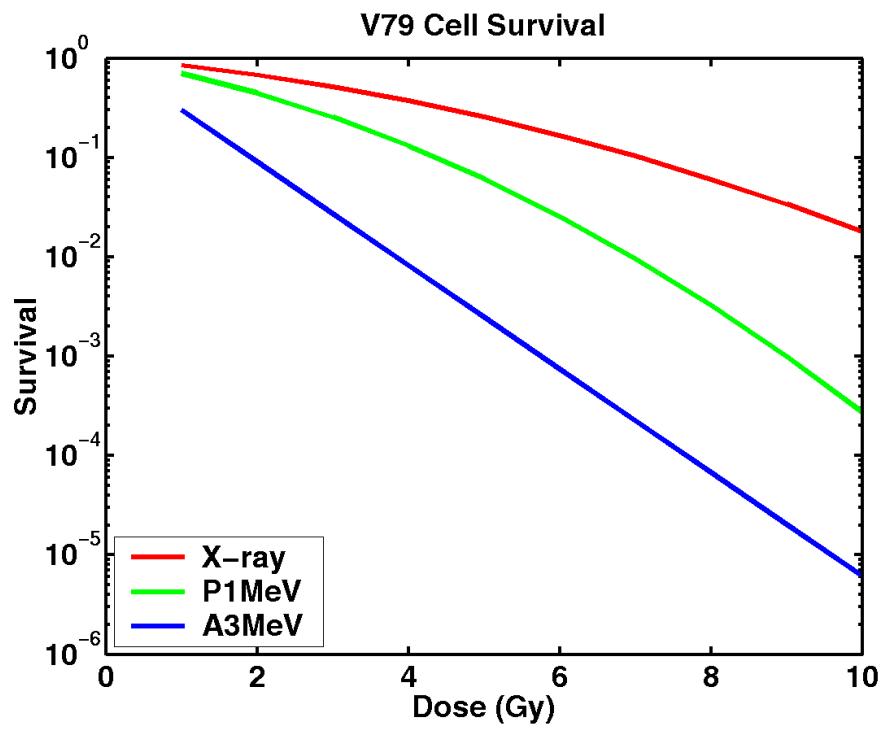
- A better way of characterizing radiation track
- Microdosimetric quantities vary with the size of target volume
- Microdosimetry is a recommended method for characterising radiation quality when biological effectiveness is not well known
- Is there a volume that is most suitable to characterize clinical RBE-values?

Example 1

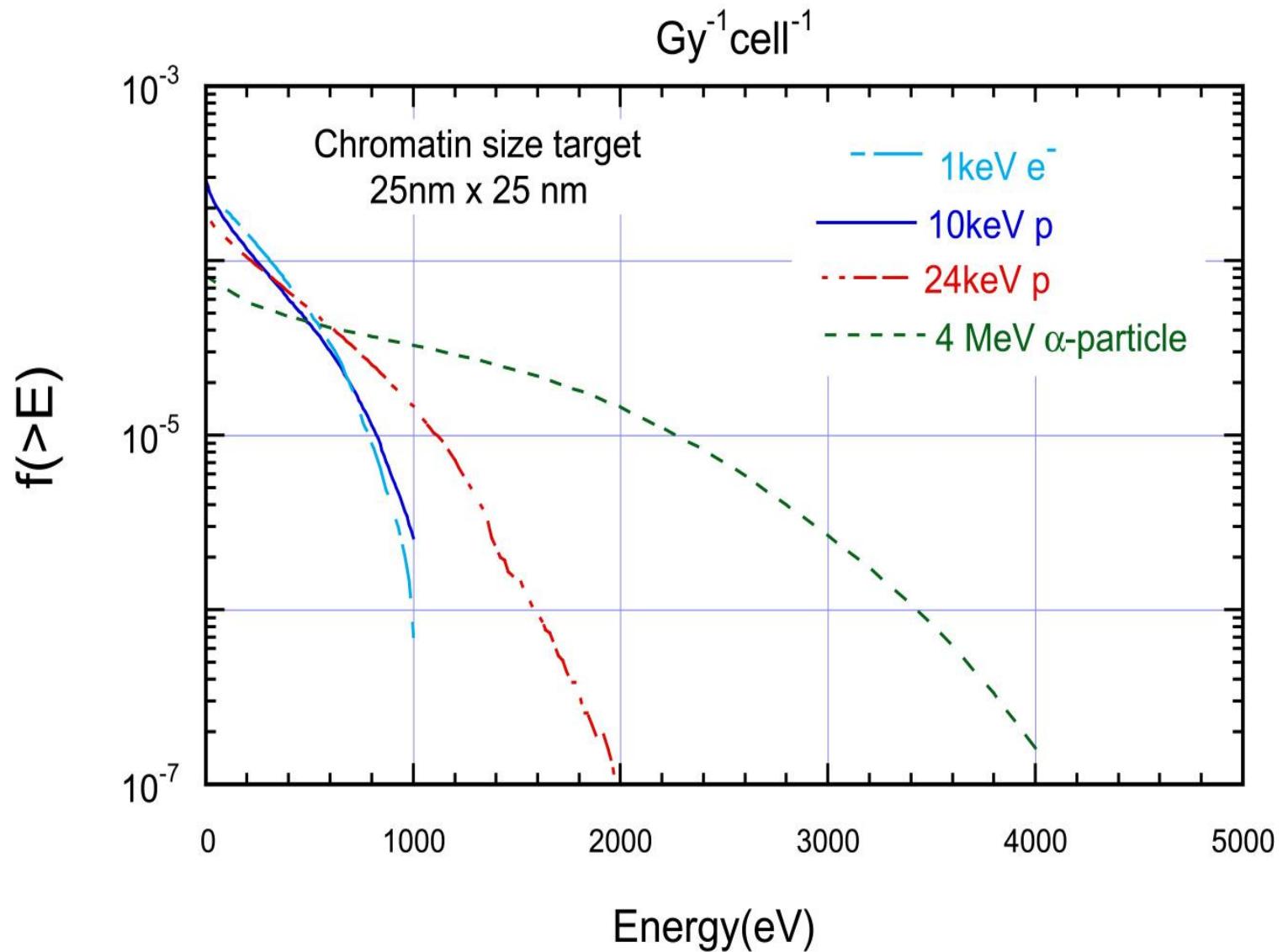
Energy deposition

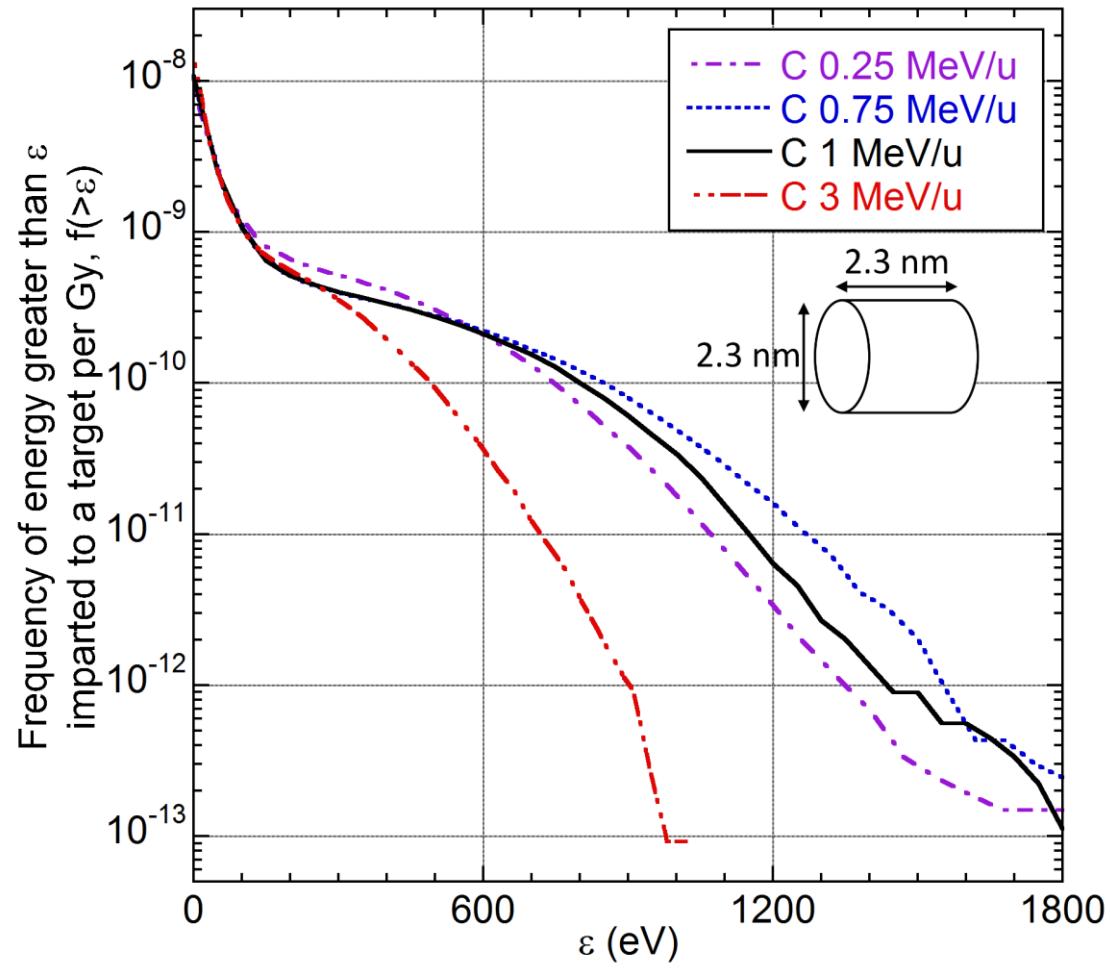


Cell Survival

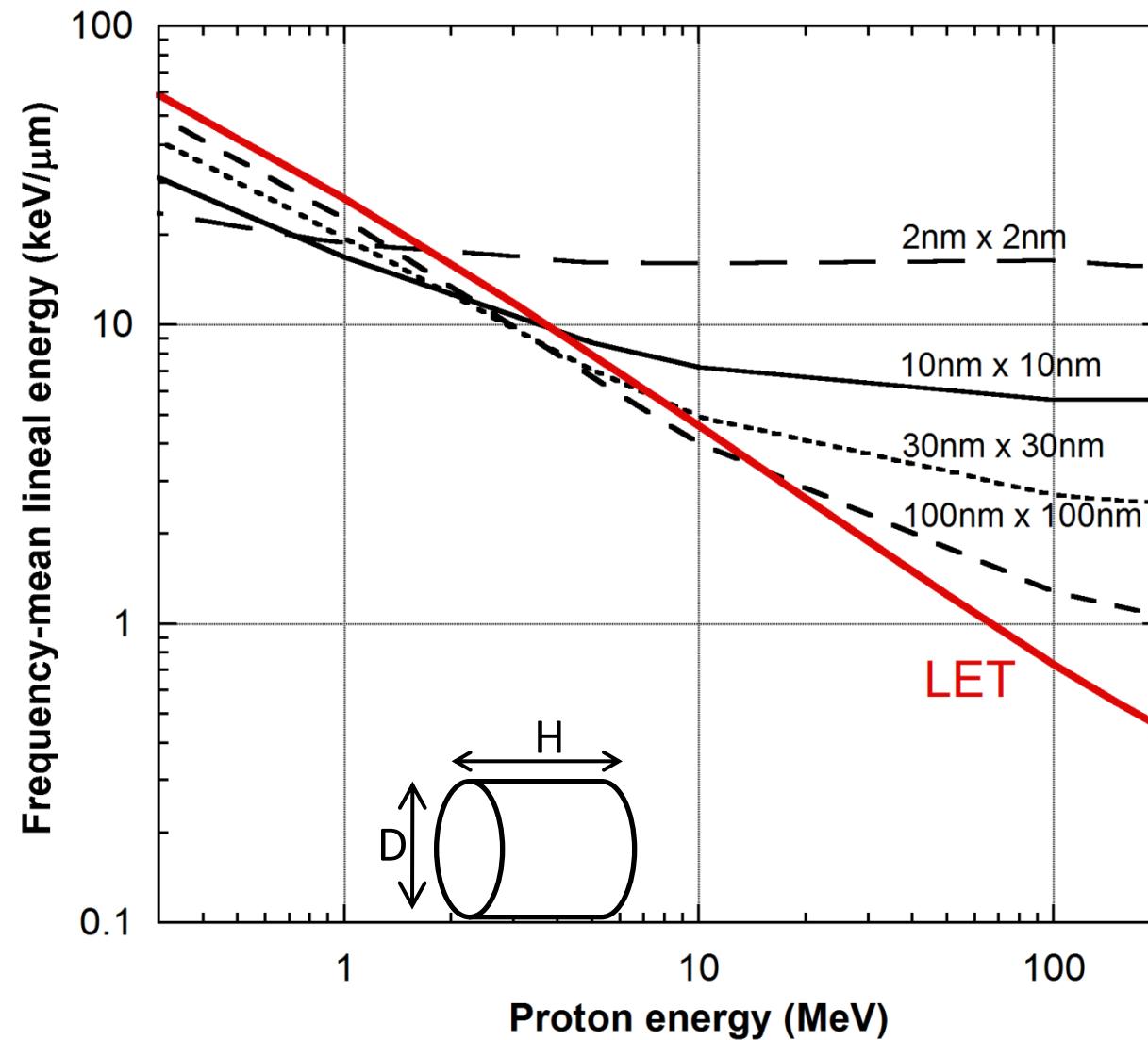


Absolute Frequency of deposition events of energy $> E$





Frequency mean lineal energy (y_F) vs. LET for protons



Lineal energy (y)
= Ratio of **energy** imparted by a single track to the mean chord length of the target

LET = Ratio of **average energy loss** of a particle in its path length

Example 2

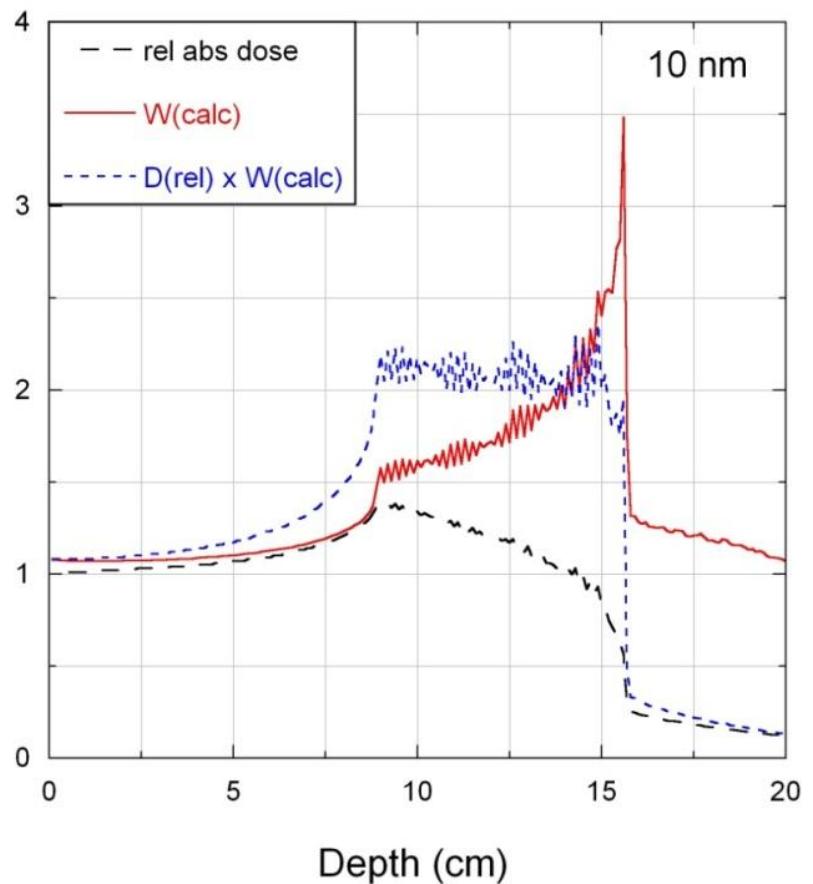
RBE v W values

Can α -ratio and y_D be correlated?

Weighting factors in Rad. Protection & Radiation Therapy

	w_R	RBE _{clin}
^{60}Co γ /X-rays	1	1.25
^{60}Co γ /Protons	2	1.1
^{60}Co γ /Neutrons	2.5 -21	3.2
^{60}Co γ / C- ions	20	3.2 ?

Why are they different?



Radiation quality	α -ratio derived from the LQ relation	y_D Ratio $D=10\text{nm}$
X-ray/ $^{60}\text{Co} \gamma$	1.2	1.16
p (175 MeV) / $^{60}\text{Co} \gamma$ in SOBP at 5cm	1.1	1.05
^{12}C SOBP / $^{60}\text{Co} \gamma$ centre	2.9	2.2
^{12}C SOBP / $^{60}\text{Co} \gamma$ distal end	3.6	3.6
$n/^{60}\text{Co} \gamma$	3.8	3.7

Conclusion1

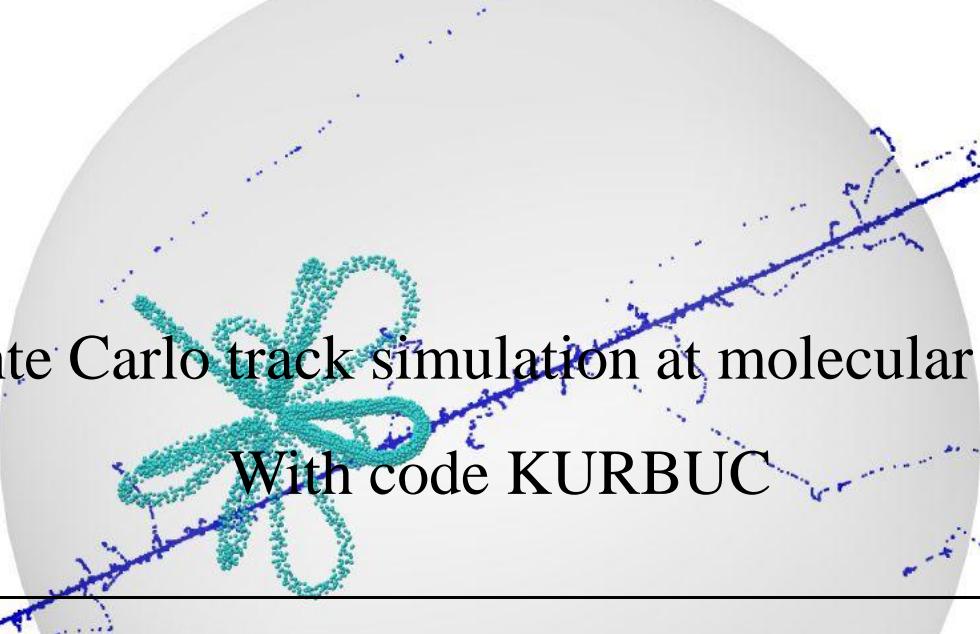
- All microdosimetry parameters and distributions can be obtained from absolute frequency of energy depositions in the target under consideration.
- We have calculated such data for electrons, and ions in target sizes 2nm – 100nm

Conclusions 2

1. Microdosimetry is a recommended method for characterising radiation quality when biological effectiveness is not well known (IAEA)
2. Size of the simulated target volume influence microdosimetric quantities.
3. For a simulated volume of about 10-15 nm, the α -ratio increases approximately linearly with the y_D ratio for all investigated radiation beams. (Lindborg et al 2013)
4. The correlation between y and α provides the evidence for the use of y to characterize therapy beam when weighting factors to be estimated
5. Low energy electrons play crucial role in characterizing radiation field

I) 4D DESCRIPTION OF RADIATION

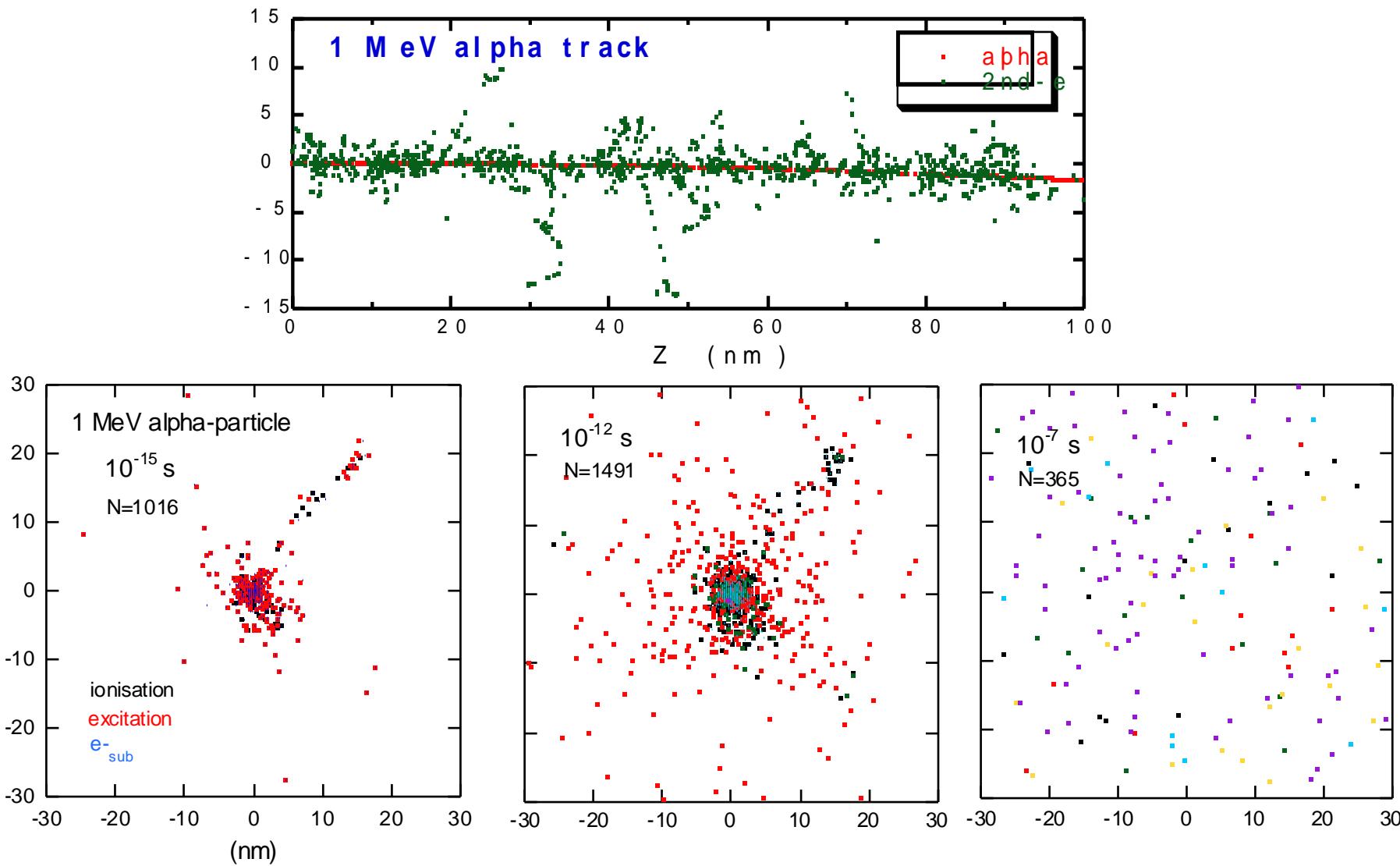
TRACK (x, y, z, t)



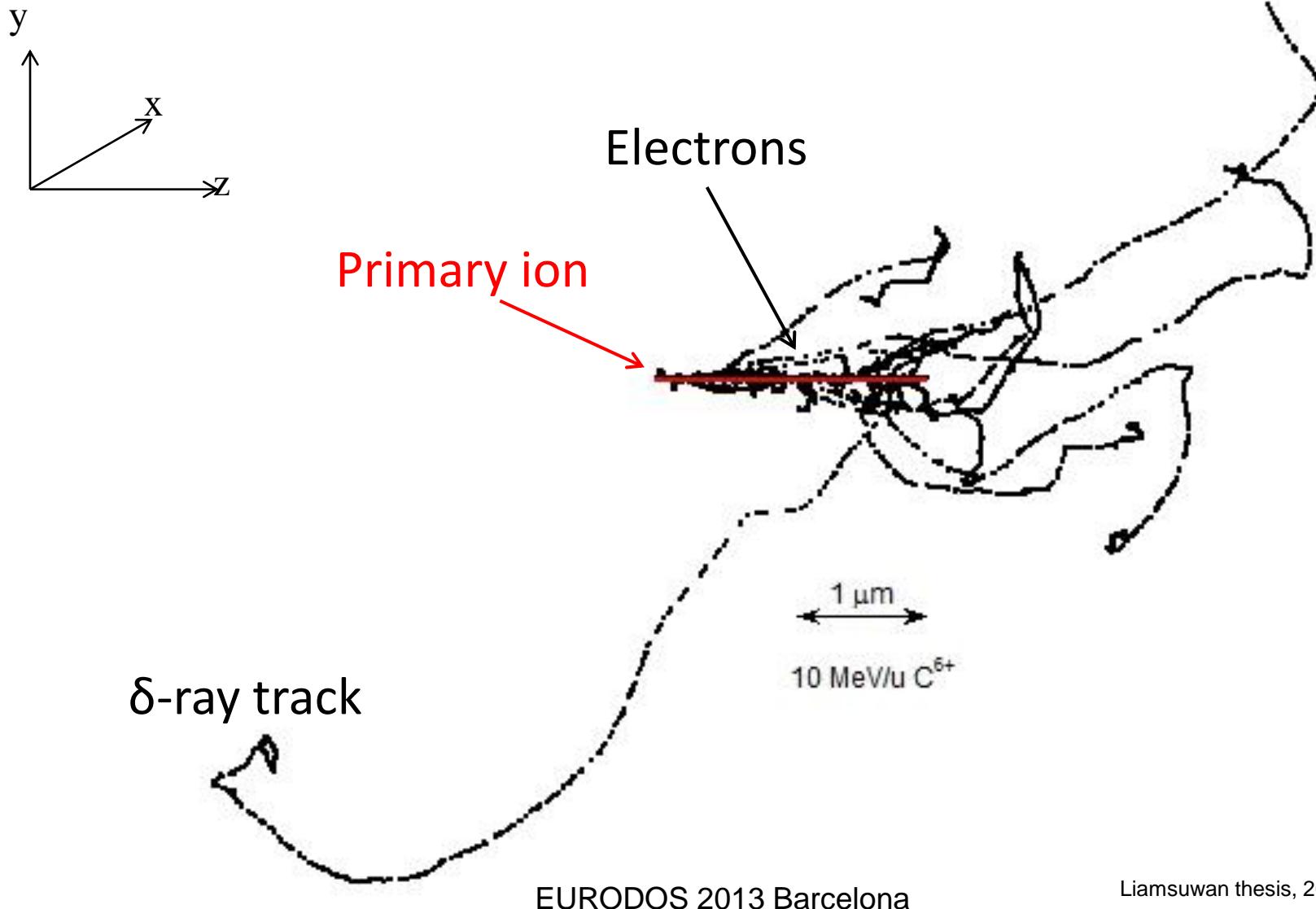
Monte Carlo track simulation at molecular level With code KURBUC

<i>Kurbuc</i>	Uehara & Nikjoo	electron	1992	10eV - 10 MeV
<i>Kurbuc_Pits99</i>	Wilson & Nikjoo	ions	1999	$\geq 0.3 \text{ MeV/u}$
<i>Kurbuc_proton</i>	Uehara & Nikjoo	protons	2001	1keV – 1MeV
<i>Kurbuc_alpha</i>	Uehara & Nikjoo	α -particles	2002	1keV/u – 2MeV/u
<i>Kurbuc_Chem</i>	Uehara & Nikjoo	chemistry	2006	$\geq 10^{-12} \text{ s}$
<i>Kurbuc_Neutron</i>	Nikjoo & Uehara	neutrons	2007	thermal - 100 MeV
<i>Kurbuc_liq</i>	Emfietzoglou et al	electron	2008	10 eV – 10 keV
<i>Kurbuc_Proton</i>	Liamsuwan et al	protons	2010	1keV – 300 MeV
<i>Kurbuc_Carbon</i>	Liamsuwan & Nikjoo	C-ions	2012	1keV/u – 10MeV/u

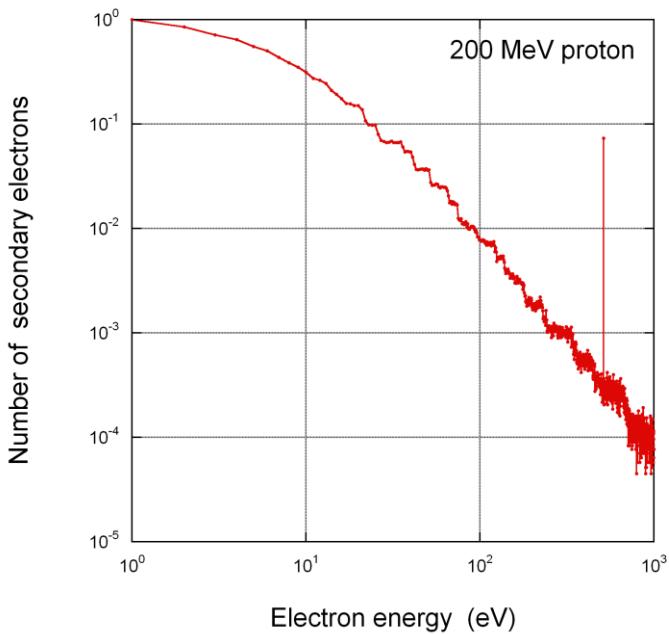
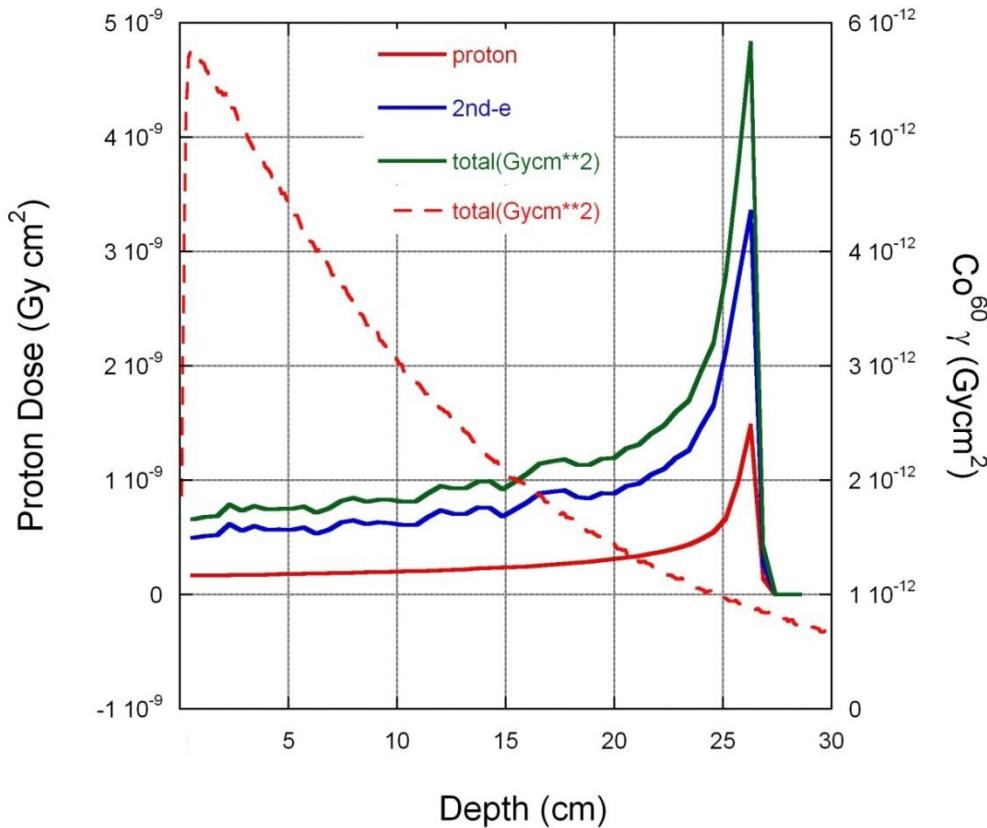
Physical and Radical Chemistry Simulation of Radiation Track at Molecular Level



Radiation track structure



MCTS simulation with sensitivity at a single cell level



Liamsuwan et al 2011, 2012
Liamsuwan and Nikjoo, 2013

Radiation	Depth at	Dose Gy cm^2	Fluence for 1 cGy / cm^2	Track # per cell Nucleus
$^{60}\text{Co} \gamma$ rays	5 mm	5.8×10^{-12}	1.72×10^9	6900
200 MeV proton	Bragg peak	4.7×10^{-9}	2.13×10^6	8.5
10 MeV/u C ions	Bragg peak	1.3×10^{-6}	7.69×10^3	0.03

Number of events in a 200 MeV full slowing down proton track

p	elastic scattering	200,908
p	ionization	1,943,795
p	excitation	1,117,797
p	e-capture	1,294
H	elastic scattering	2,259
H	ionization	1,084
H	excitation	676
H	electron loss	1,293
<i>Secondary electrons</i>		
ionization (12.62 eV)	12.62 eV	1,977,465
ionization (14.75 eV)	14.75 eV	1,494,653
ionization (18.51 eV)	18.51 eV	877,941
ionization (32.40 eV)	32.40 eV	20,812
ionization (539.7 eV)	539.7 eV	7,135
excitation	A ₁ B ₁	198,989
excitation	B ₁ A ₁	648,345
excitation	Rydberg A+B	246,620
excitation	Rydberg C+D	347,007
excitation	diffuse band	1,204,030
excitation	H* Lyman a	343,570
excitation	H* Balmer a	67,931
excitation	OH*	836,387
sub-excitation electrons		634,450

Some physical characteristics of radiation tracks

Particle type	Energy (keV)	primary interactions (%)	secondary electron interactions (%)	dE/dx (keV/ μm)	Energy in track by primary %	Energy in track by delta electrons %
e ⁻	1keV	25	75	12	39	61
e ⁻	10keV	23	77	2.3	37	63
e ⁻	100keV	22	78	0.42	34	66
Proton	1MeV	21	79	27	30%	70%
Proton	20MeV	20	80	2.5	34%	66%
Proton	200MeV	20	80	0.4	30%	70%
Carbon	20MeV/u	20	80	93	20%	80%

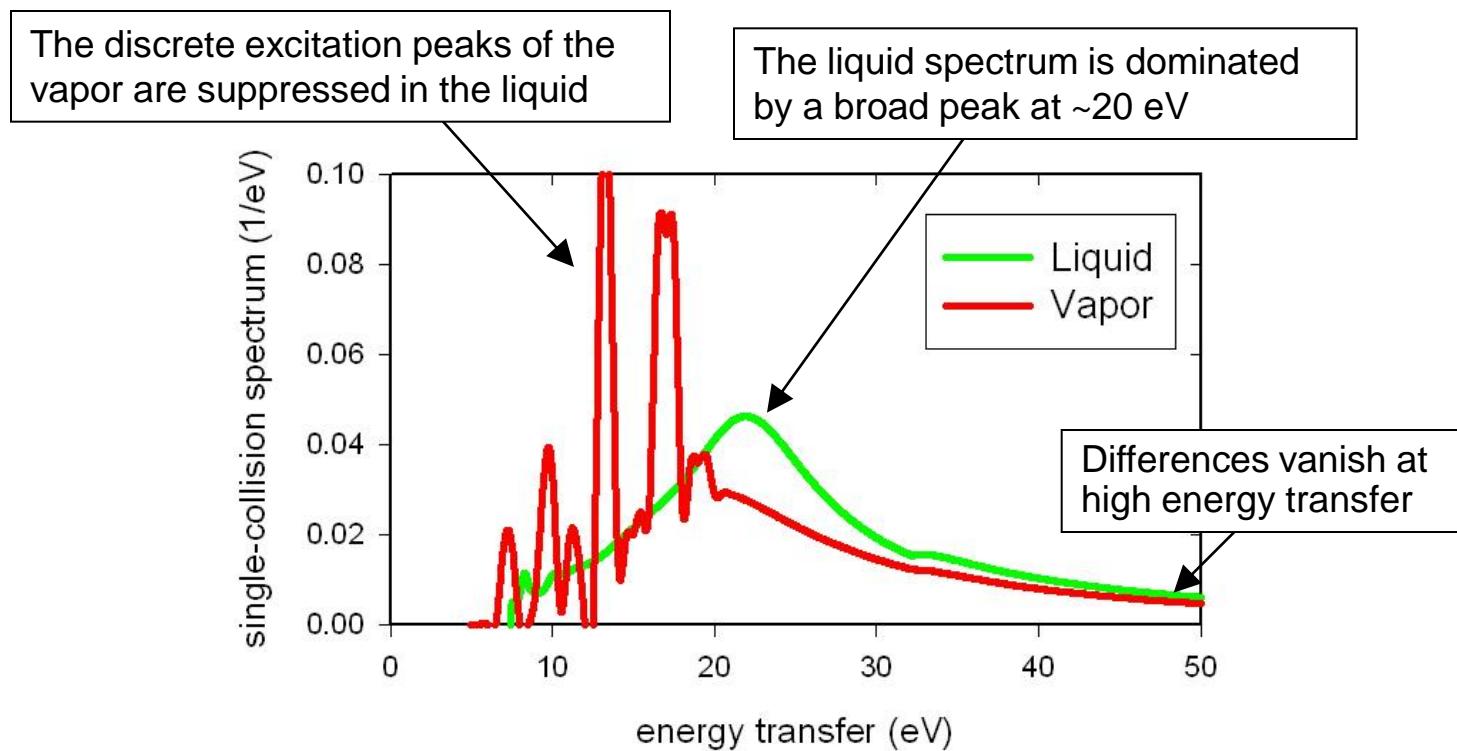
Conclusions 3

- Radiation track description in space and time is possible for electrons and ions in homogenous biological media
- How good is the technology?

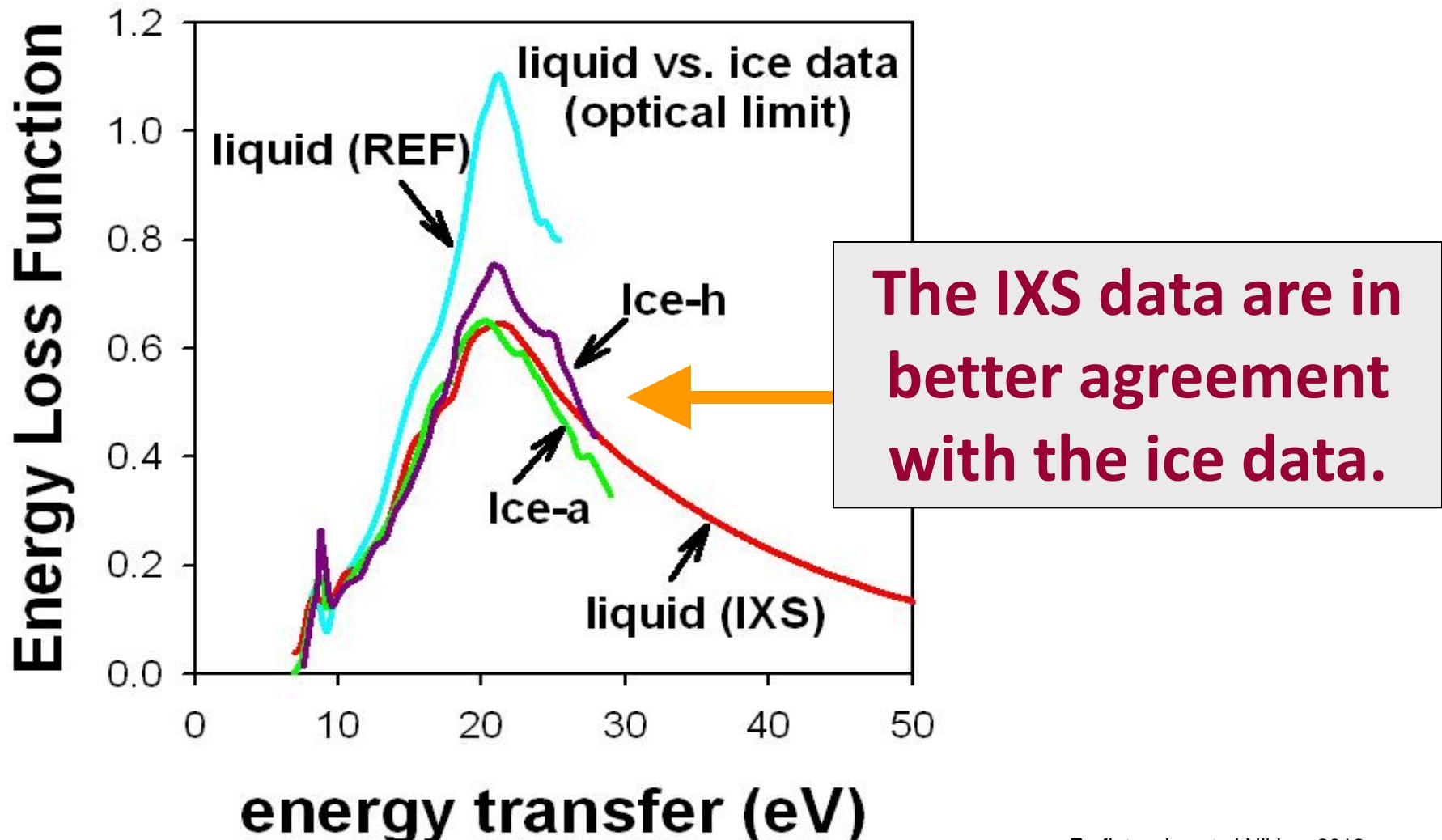
Electron energy loss in condensed matter

- Inelastic interactions with atomic electrons leading to *electronic excitations (including ionizations)* is the most important energy-loss mechanism for electrons at all energies of practical interest.
- Electronic excitations depend not only upon the atomic composition of the system but also upon its state of aggregation (gas vs. solid or liquid).

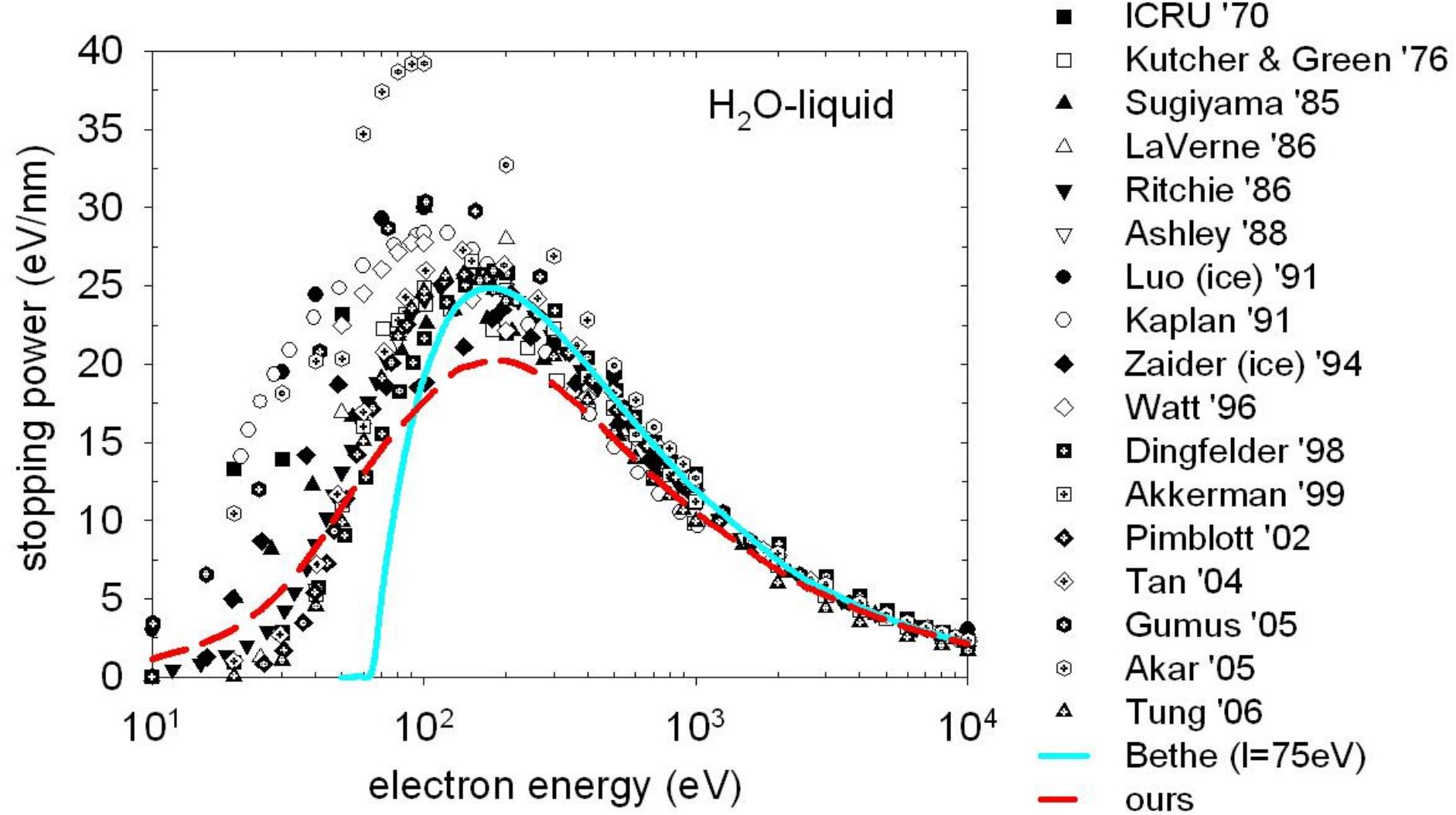
Example: single-collision energy-loss spectrum of vapor vs. liquid water



Liquid vs. Ice data



Electron stopping power in liquid water



Conclusions 4

physics of electron energy loss in liquid water

- For electrons >200 eV optical-data model calculations for the IMFP are not very sensitive to the choice of the physics model used
 - The differences between models are less than $\sim 10\%$
- For electrons <200 eV the IMFP is very sensitive to the choice of physics model

Conclusions 4

Is Trajectory Simulation Correct?

An explicit trajectory picture of the transport of low energy (< 1 keV) electrons in liquids and amorphous solids is certainly not valid according to the Heisenberg uncertainty principle. In fact, it does not correspond to physical reality.

But, a trajectory treatment provide a good approximation of multiple quantum scattering down to electron energies in the order of ~ 10 eV, due to the incoherence introduced by a randomlike structure of the medium and to the presence of multiple inelastic scattering.

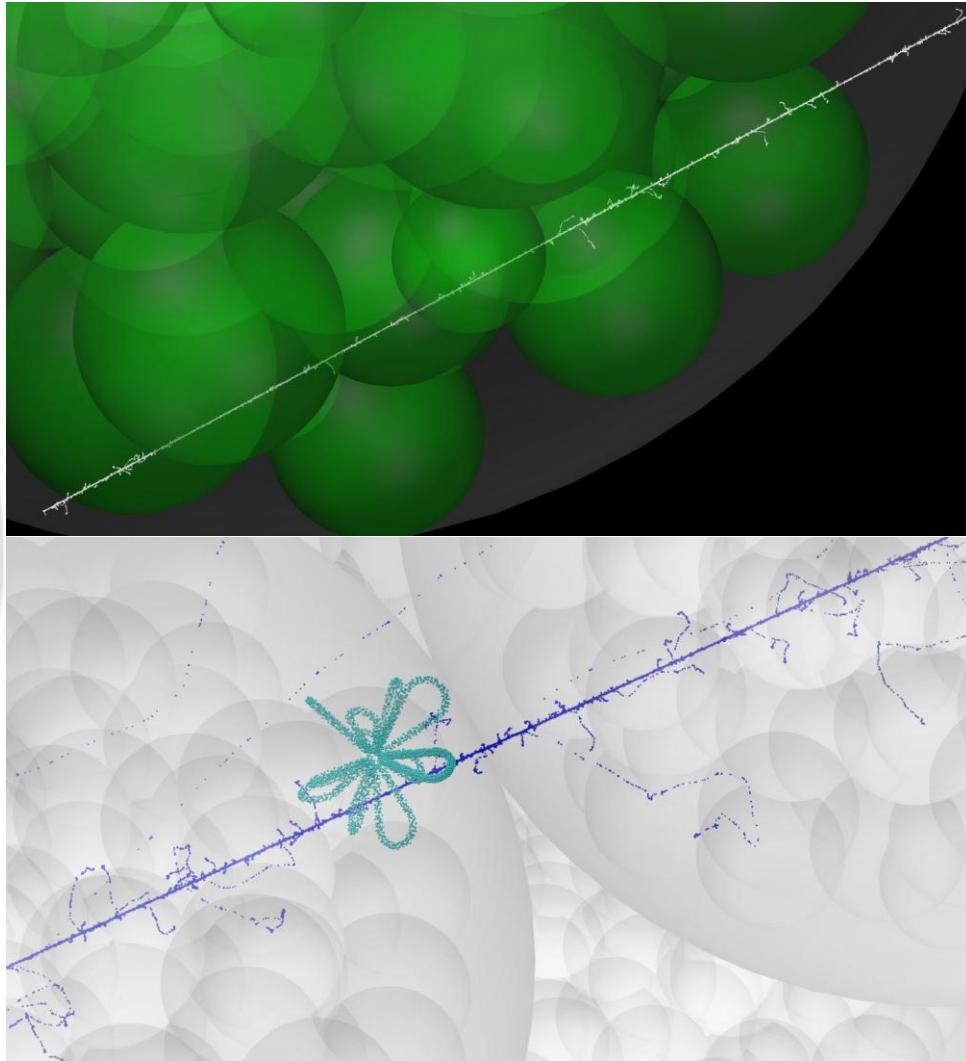
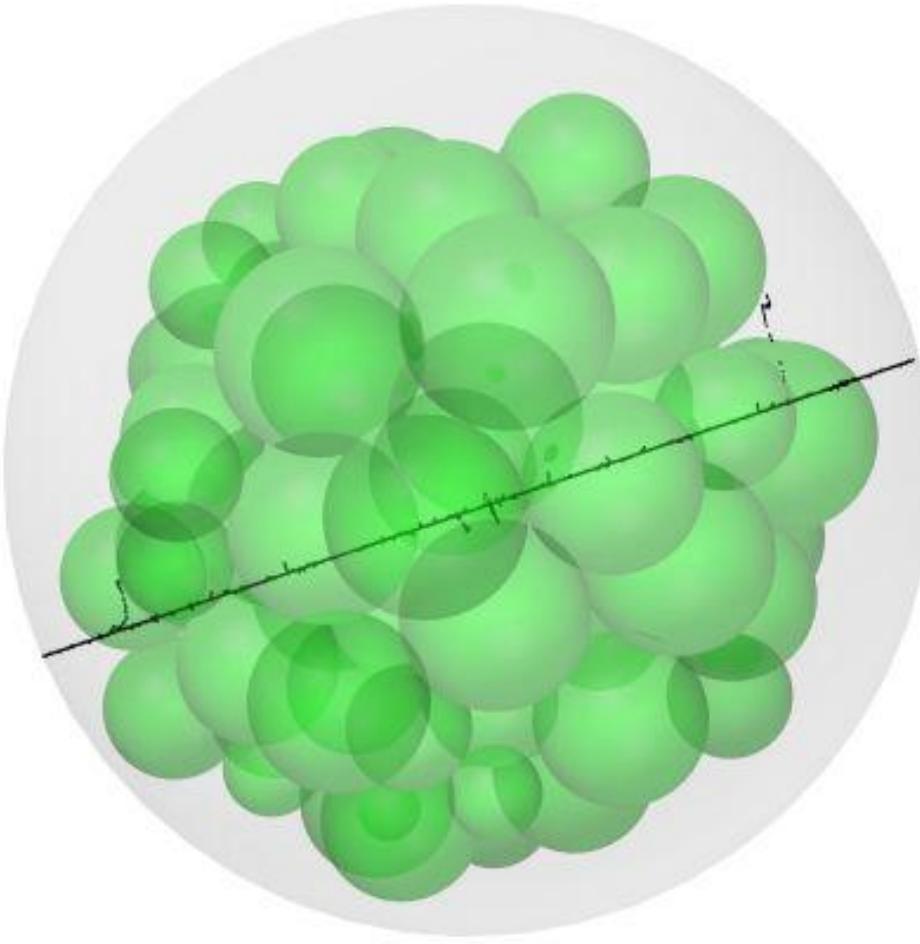
Conclusions 5

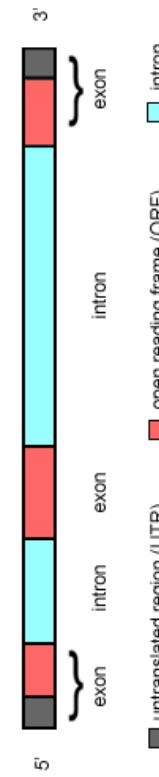
- a. We now have the technology to describe physical and chemical interactions of electrons and ions at molecular level. (track segment and full-slowing down)
- b. Low energy electrons <100eV are responsible for most of energy depositions by a track
- c. Although we know a lot about physics of radiation track but at energies below 100eV our understanding is incomplete and uncertain, especially in condensed matter
- d. Microdosimetry considerations proves LET is not a good parameter for characterising radiation track

II) DNA DAMAGE

DNA Damage in human genome

Intersecting domains:
70, 44, 18, 13, 20





Goorely , Terrissol,
Nikjoo 2008

30 nm fibre loops
from a 'factory'

'hprt'
gene

exons

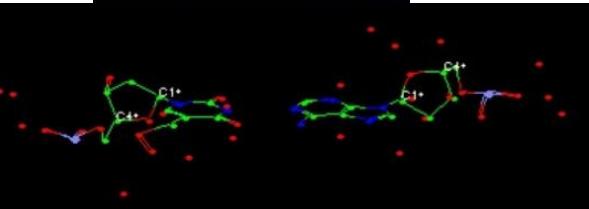
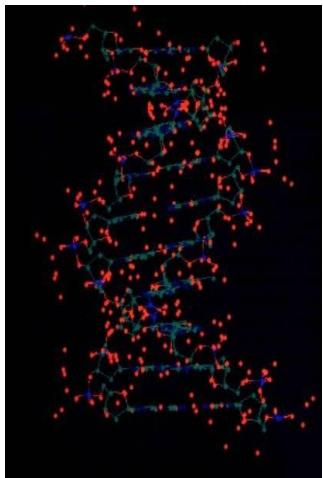
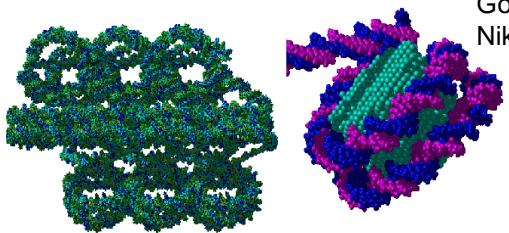
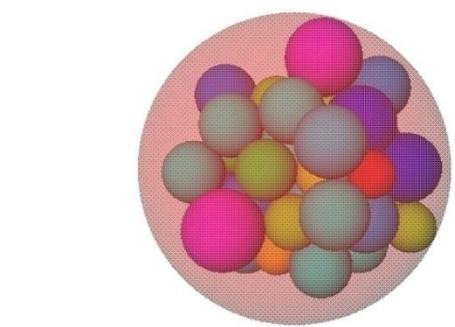
HPRT gene ~ 40 kbp

<1 loop> ~ 86.5 kbp ~ 5×10^6
atoms

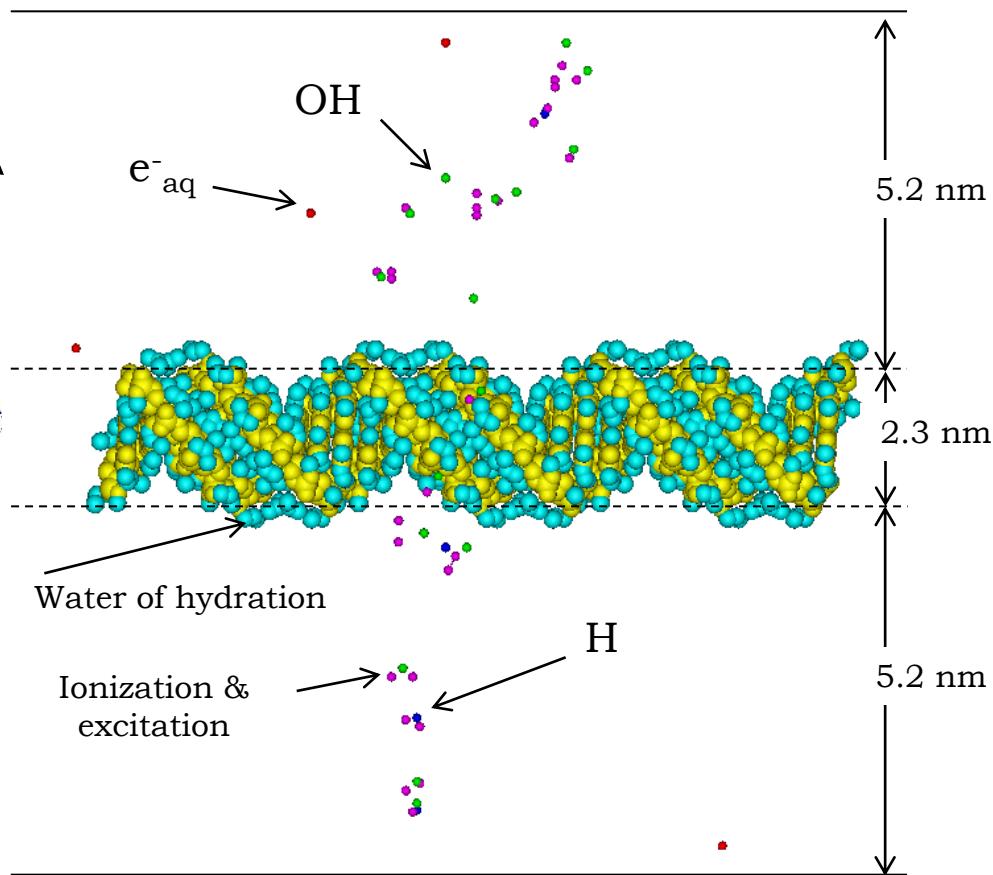
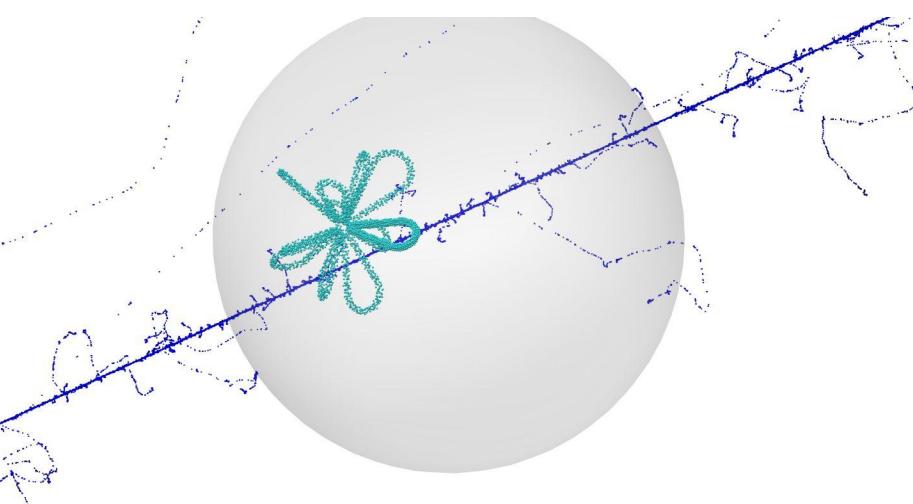
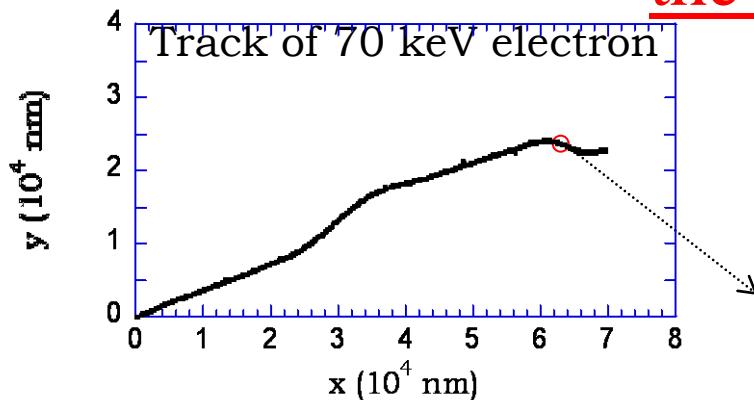
EURODOS 2013 Barcelona

1 factory ~ 50×10^6 atoms

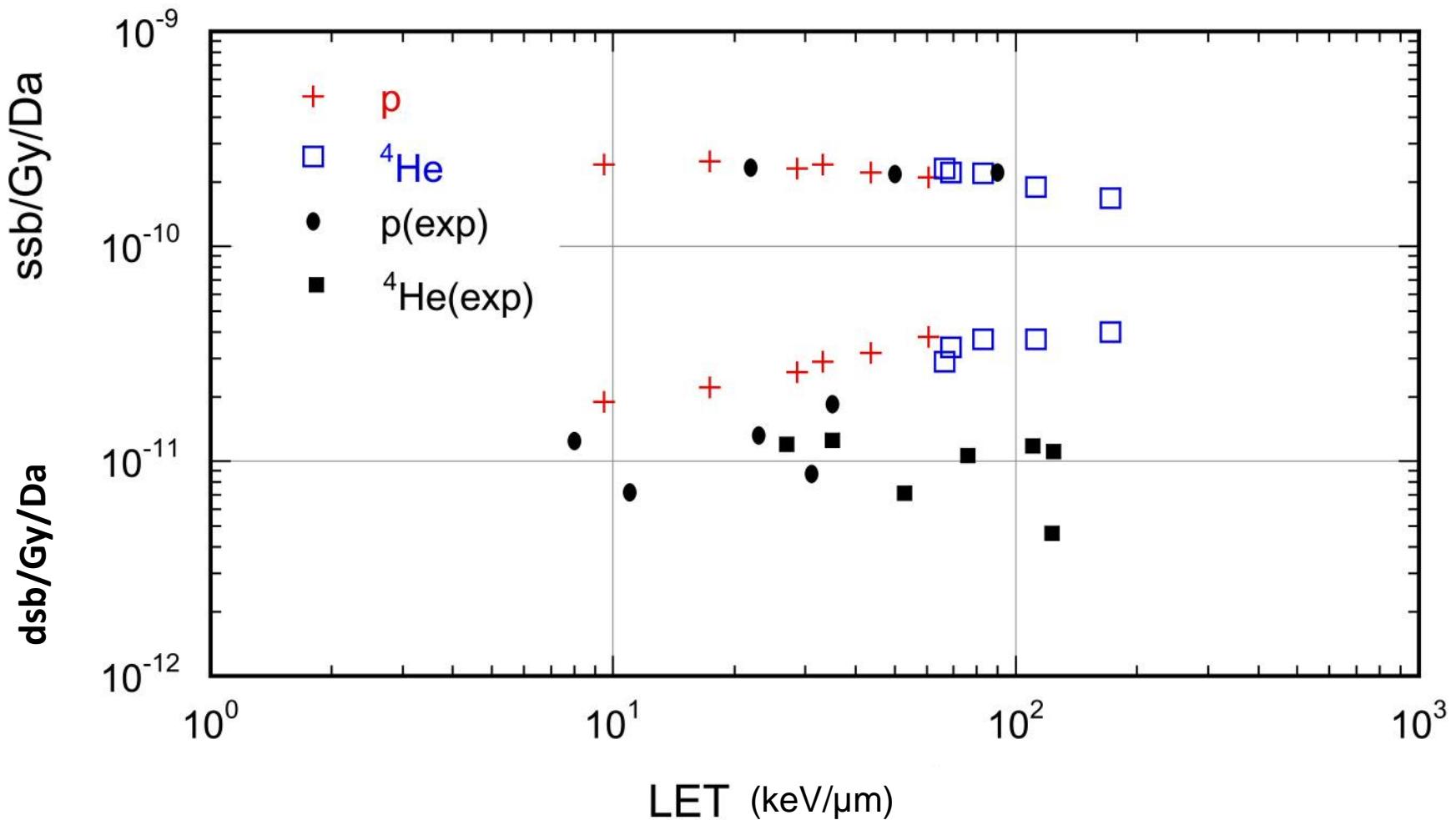
Nikjoo, Girard, 2012



Cell Response to Radiation: I- track interaction with the genome



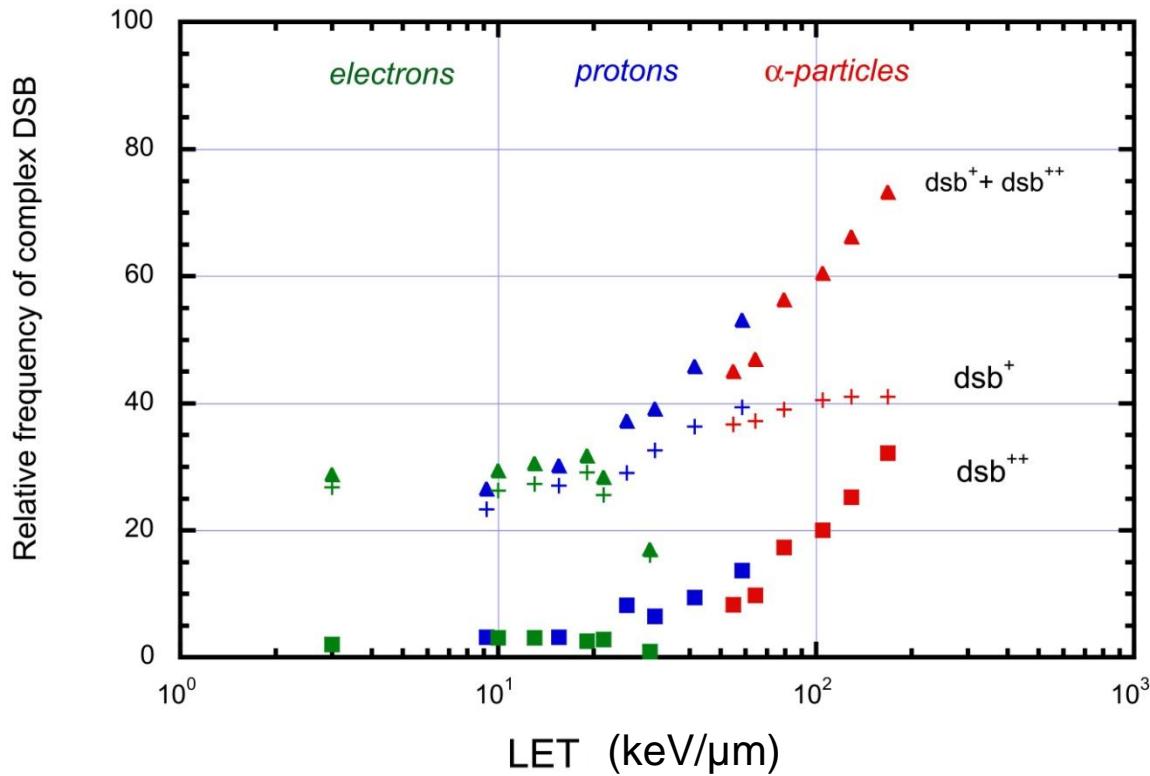
Cell Response to Radiation: Yield of SSB & DSB



EURODOS 2013 Barcelona

Charlton, Humm, Nikjoo, 1989
Nikjoo *et al*, 2001

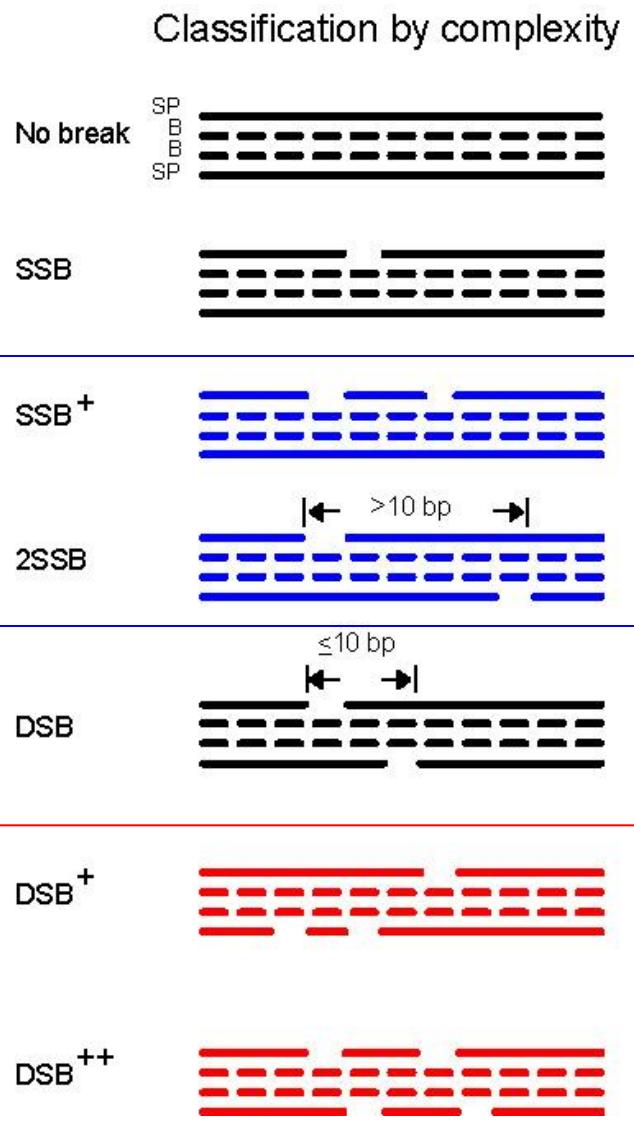
Cell Response to Radiation: Complexity of DSB



Charlton, Nikjoo, Humm, 1989
Nikjoo *et al* 1999
Nikjoo *et al* 2001
Sankaranaranan & Nikjoo, 2011
Taleei & Nikjoo 2012, 2013

Low-LET
Complex DSB ~20%

High-LET
Complex DSB ~70%



SSB, DSB, & BD in cell nucleus from a single track of 0.5 MeV/u proton

TOTAL ENERGY = 178. TRACK: 1, DOMAIN: 10, FACTORY: 115, LOOP: 6
00276 43609 43642 46495

[x = SSB]
[1 & - not an SSB]

TOTAL ENERGY = 331. TRACK: 1, DOMAIN: 3, FACTORY: 124, LOOP: 9

00394	00480	00529	00575	00604	01426	01513	01610		79795
.	x..x	1	1...1
x	1	1	1	x..	x...
.	.. x.
.	.. x.	.	.	1...x	.	.1-	-

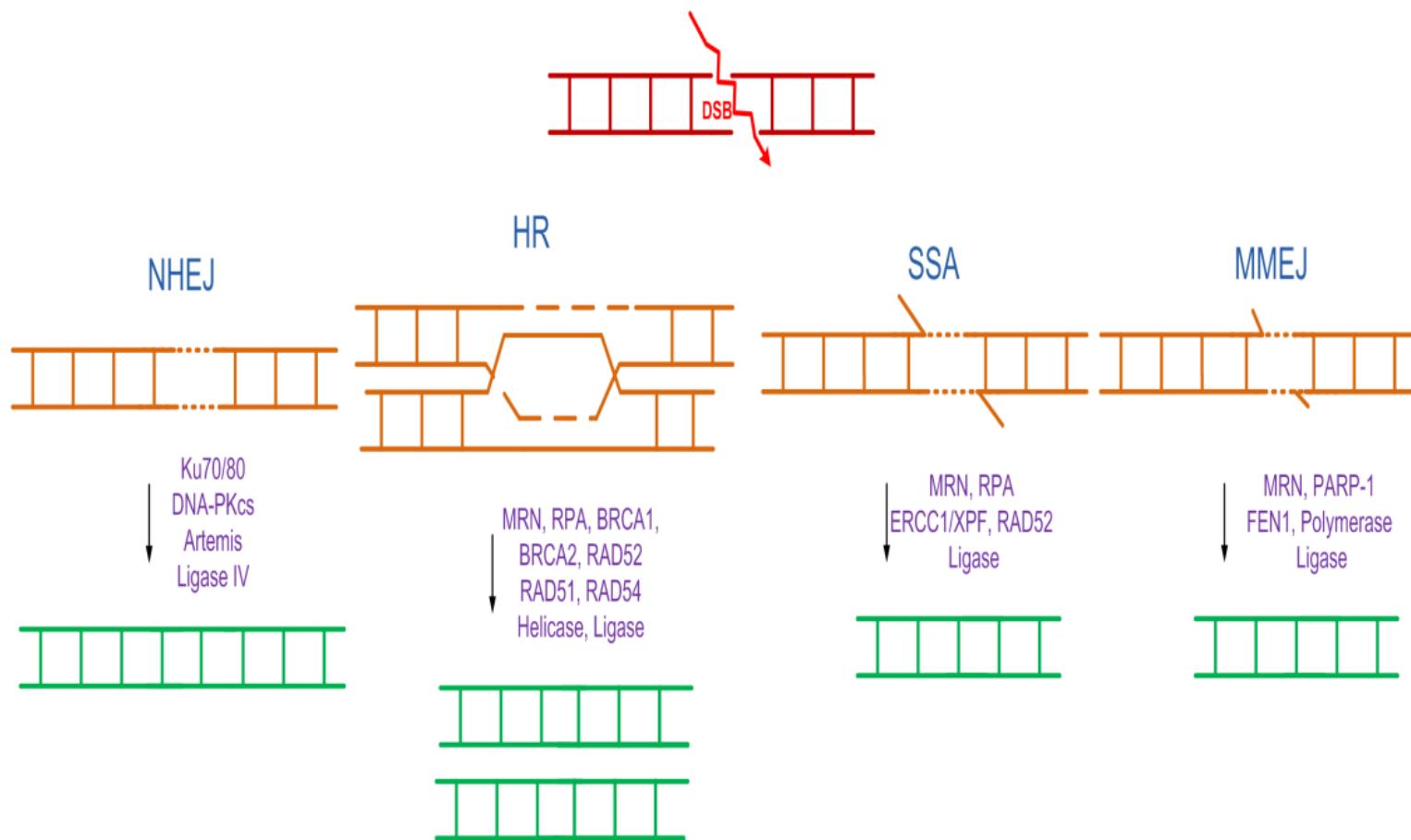
TOTAL ENERGY = 179. TRACK: 1, DOMAIN: 3, FACTORY: 125, LOOP: 9

00802	01662	01959		03089	04140	04172		05255	05283	06381
.	1	-.	1.	-.	.	.
.	-.	-.	.	1
.	.	.	.	1.	-.	.	.	.	-.	.
x	1	1.	.	-1	.	-.	.	.	1	-.

TOTAL ENERGY = 94. TRACK: 1, DOMAIN: 90, FACTORY: 28, LOOP: 11
01661 01756 02445 02592 02672

.	-
.	.	.	X.....	.
.	.	X	...-	.
1X-	

DSB-Repair Kinetics



Kinetics of Repair by NHEJ (C_K X-ray)

Initial damage spectrum

TCGCGCGAATT CGCGCGAATT CGCGCGAATT CGCGCGAATT CGCGCGAATT CGCGCGAATT CGCGCGAATT CGC
... ID I
I. I I
... D I I I II I
... I I I

Biochemical repair of initial damage	Elapsed Time (min)	Elapsed Time (Average DSB _c)
Ku70/80 finds the DSB ends and translocates inward	0.3	0.3
DNA-PKcs is recruited to the damage site	1.3	1.5
First autophosphorylation of DNA-PKcs	4.3	4.4
Second autophosphorylation of DNA-PKcs	7.8	7.6
End processing by Artemis	187.3	184.1
Gap filling by Polymerase λ - μ	339.5	300.9
Ligation of complex DSB	391.9	348.7
Repair time (min) for complex damage	391.9	348.7

Radiation Biophysics Group (RBG)



Hooshang Nikjoo, Professor, Group Leader

Peter Girard

Radioprobing/Molecular computational studies



Reza Taleei

DNA Damage-Repair



Thiansin Liamsuwan

Physics and track simulation



Lennart Lindborg

Microdosimetry



Alfredo Metere

Genome Technology/IT



Shirin Rahmanian

DNA damage response & repair



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